

Research Paper

Combination of PET and CXCR4-Targeted Peptide Molecule Agents for Noninvasive Tumor Monitoring

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Abstract

Precision medicine is emphasizing not only at individual but also at disease molecule level in modern medicine. Therefore, target-specific molecular agents are crucial for precise diagnosis and treatment. We developed a peptide agent that binds a critical chemokine receptor-CXCR4 and could be used to detect tumor status. Confocal images showed binding of the peptide agent to human osteosarcoma cells. Clinical gold-standard molecular imaging agent PET showed tumors had high glucose metabolism, CT showed that these xenograft tumors were calcified and displayed hypervascularity. Peptide imaging demonstrated that these tumors were CXCR4 positive. However, Western blot protein analysis revealed a discordance between the tumor and the CXCR4 targeted agent, suggesting that small changes in peptide sequences have profound effect on binding to their targets. We also demonstrated the molecular screening by modifying the peptide sequence and thereby altering the binding properties of the agent. In conclusion, this study demonstrates that small molecule peptide agents can be used as an additional diagnostic tool for precision medicine.

Key words: optical imaging, peptide imaging, CXCR4, osteosarcoma, molecular imaging

Introduction

Personalized medicine promises to deliver individualized treatments that are tailored to the genetics, RNA, proteins, and metabolites of each patient's disease [1]. These advances in personalized medicine have the potential to increase the quality of patient care for numerous diseases. For cancer chemotherapy, precision medicine entails administering target-specific agents, including microRNA and antibodies, to a target-positive disease at properly timed and effective biological doses while minimizing systemic toxicity. Successful therapy requires an understanding of ongoing changes as tumors progress and respond to treatments [2]. Therefore, it is crucial to develop new tools, such as noninvasive molecular imaging, for acquiring accurate information about the tumor status [3].

Labeling target-specific agents with imaging reporters offers a tool for repeated and noninvasive

evaluation of tumor status. Currently, the molecular imaging agent most commonly used in clinical practice is ¹⁸F-fluoro-deoxy-glucose (¹⁸F-FDG). Therefore, it is crucial to develop molecular imaging agents that match the targets of precision medicine.

Among the molecular targets, cytokines and chemokines are important intercellular signals in inflammation, immunity, and tumor and endothelial cell processes. These factors have therapeutic potential when exogenously delivered either alone or in combination with biological or chemotherapeutic agents [4-6]. CXCR4 is a chemokine receptor that belongs to the large family of G protein-coupled receptors. CXCR4 plays a crucial role in a number of biological processes, including the trafficking and homeostasis of immune cells such as T lymphocytes. In addition, CXCR4 has been reported to be a prognostic marker in various types of cancer,

including leukemia, lung, breast, stomach, pancreas, and prostate cancer [7-11]. CXCR4 is highly expressed on cancer stem cells and plays a crucial role in metastasis to the brain, lymph nodes, lungs, liver, and bone [11, 12]. The metastatic functions are reported through CXCL12 and its receptor CXCR4 [13-18]. Therefore, CXCR4 could be a therapeutic target for tumor progression, angiogenesis, and metastasis, and CXCR4 targeted treatments have the potential to improve overall patient survival [19].

In this study, we developed a peptide-based, CXCR4-targeted agent labeled with a near-infrared (NIR) dye. In cell based studies, we demonstrated that these peptide agents bind to CXCR4 positive human osteosarcoma cells. Whole-body optical imaging demonstrated high NIR signal intensity within CXCR4-positive tumors and CXCR4-positive tissues, suggesting that synthetic peptide agents could be used to evaluate CXCR4 chemokine receptor status in preclinical studies. Furthermore, we demonstrate that target-specific molecular agents can be used with current imaging technologies (^{18}F -FDG PET, CT, or MRI) to noninvasively monitor disease status. The techniques developed here may be useful in developing additional targeted therapeutic agents for personalized medicine.

Results

NIR-labeled CXCR4 agent binding

In an *in vitro* binding assay, no detectable NIR signal was emitted from the Saos-2 cells incubated with free NIR dye (Fig. 1A1, B and C) and the NIR signal intensity was near background levels in a

quantitative 3D plot (Fig. 1D). There was no detectable signal when CXCR4 agent co-incubated with CXCR4 negative nasal cancer cell SUNE-1 (Fig. 1A2). In contrast, the NIR-labeled CXCR4 agent bound to the all of the osteosarcoma cells when processed in parallel (Fig. 1E-F). Merged images of the NIR signal, the cell nuclei, and the differential interference contrast (DIC) confirmed that the NIR signal did not colocalize with the cell nucleus (Fig. 1F). The uneven intensity of the NIR signal in single cell images and in corresponding quantitative signal intensity plots suggests that the peptide agent may bind to CXCR4 in specific compartments within the cell (Fig. 1G-H).

In vivo molecular imaging

Using the NIR-labeled CXCR4 agent, an increase in NIR signal intensity in osteosarcomas xenografts could be detected in subcutaneous model as early as 7 days after the inoculation of Saos-2 cells. NIR imaging illustrates the binding of the CXCR4 agent within the tumor, as well as known CXCR4-positive tissues, including the thymus and liver (Fig. 2A). Tumor-to-background ratios ranged from 1.01 to 1.75 during a 48-hour period (n=8). Whole-body CT imaging confirmed the size and location of the tumor (Fig. 2B). Skeletal CT imaging demonstrated calcification of the tumors and revealed that the bony component of the tumor had invaded beyond the tumor mass (Fig. 2C). ^{18}F -FDG PET imaging demonstrated high glucose metabolism within the center of the tumor (Fig. 2D). Merged ^{18}F -FDG PET and skeletal CT images illustrated the anatomical relationship between the tumor, glucose uptake, and calcification (Fig. 2E-F). Merged vasculature contrast

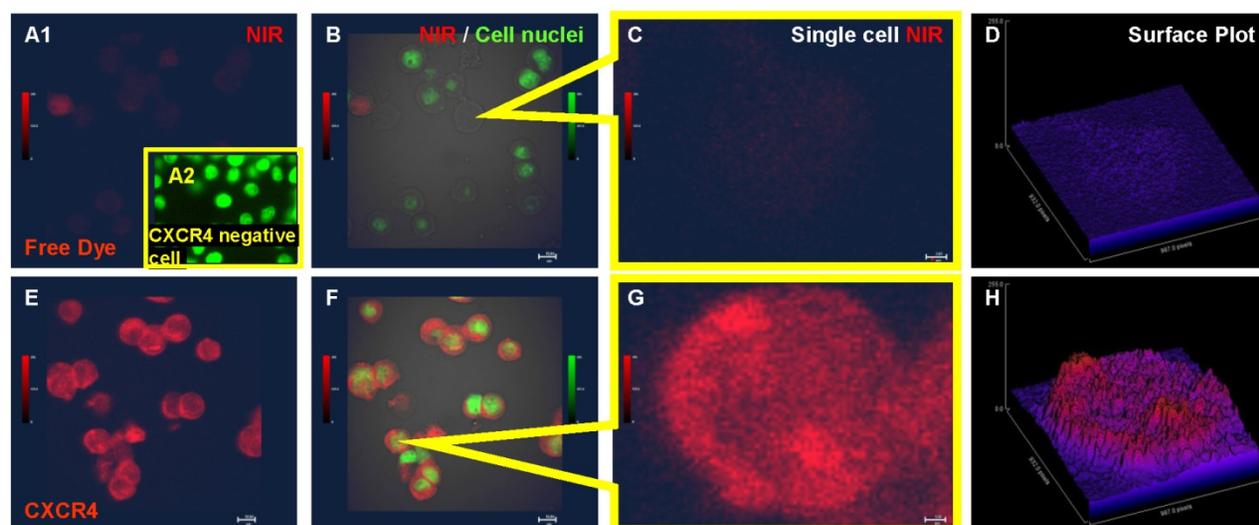


Figure 1. Confocal images demonstrating uptake of the CXCR4 peptide agent by human osteosarcoma cells. **A.** Saos-2 cells incubated with free near-infrared (NIR) dye. **B.** Merged image of the NIR signal, cell nuclei, and bright field shows cell morphology and lack of NIR signal. **C.** High-magnification image of free NIR dye uptake by a single cell. **D.** Quantitative 3D plot of the NIR signal intensity showing free dye signal near background levels. **E.** NIR-labeled CXCR4 agent binds to Saos-2 osteosarcoma cells. **F.** Merged image of the NIR signal on the CXCR4 agent, cell nuclei, and bright field. **G.** High-magnification image of a single cell binding to the NIR-labeled CXCR4 agent. **H.** Quantitative 3D plot of the NIR signal showing the CXCR4 agent bound to a single cell.

and skeletal CT images show the hypervascularity of the tumor (Fig. 2G). Finally, high-magnification optical NIR images demonstrate the binding strength of the CXCR4 agent within the tumor (Fig. 2H).

Peptide sequence alteration analysis

The sequence of the NIR-labeled CXCR4 binding peptide (agent 425) was altered and these new agents were compared in a cell-binding assay (Figure 3). The optical signal intensities of the different peptide sequences and structural alterations are presented at the same scale (B1 to B6) and merged with cell nuclei (B7 to B12). Agents 51 (B1 and B7), 423 (B2 and B8), and 429 (B6 and B12) are peptides with different sequences from agent 425 (B3 and B9). Agent 425 was modified with a radio-chelator to generate agent 427 (B4 and B10) and then further coupled with an isotope to produce agent 427-cu (B5 and B11). The altered cell binding of these agents confirms that changing the peptide sequence, adding a radio-chelator, or coupling to an isotope affects the agent binding and signal intensity of the NIR label.

CXCR4 expression in tissues

To validate our whole-body imaging results, we dissected the organs exhibiting high NIR signal intensity (thymus, liver, and tumor) and muscle tissue

as a negative control. Hematoxylin and eosin (H&E) staining confirmed the tissue origination (Fig. 4A). As an additional negative control, we harvested tissues from mice bearing CXCR4-negative nasal tumors. By Western blot analysis, high CXCR4 expression was detected in the liver of both CXCR4-negative and positive tumor xenografts (Fig. 4B, lanes C and E). Surprisingly, the CXCR4 antibody did not detect CXCR4 expression in either tumor lysate (lanes A and G) or the muscle negative control (lanes B and F). However, a higher molecular weight CXCR4 protein was detected only in the thymus and liver of mice bearing the CXCR4-positive tumor xenograft (lanes D and E), suggesting that the peptide-imaging agent and CXCR4 antibody have species- and tissue-specific binding properties.

Discussion

One of the current goals of our research is to develop molecular imaging agents as tools to validate disease targets. Such direct visualization could be used to evaluate disease markers and provide the information necessary for developing personalized treatment plans using biological target-specific therapeutic agents. CXCR4 is an important therapeutic target in many diseases and several CXCR4 antagon-

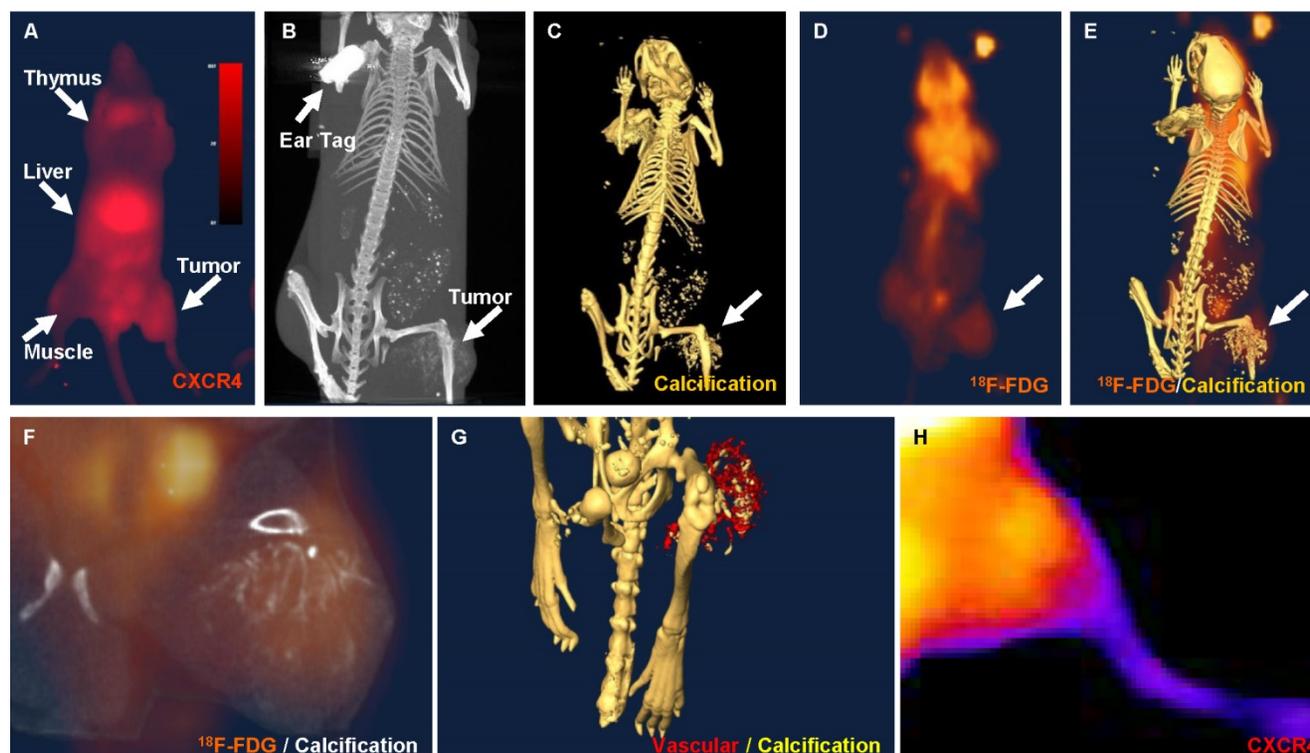


Figure 2. *In vivo* images of osteosarcoma xenografts in nude mice. **A.** NIR image showing the distribution of CXCR4 agent in the thymus, liver, and tumor. **B.** Whole-body computed tomography (CT) image showing the location of the tumor. **C.** CT image of the skeleton demonstrating calcification in the tumor region (arrow). **D.** ^{18}F -fluoro-deoxy-glucose positron emission tomography (^{18}F -FDG PET) image showing high glucose metabolism in the tumor region (arrow). **E.** Merged CT and ^{18}F -FDG PET images showing the anatomical distribution of the ^{18}F -FDG-PET signal. **F.** High-magnification of merged CT and ^{18}F -FDG PET images showing calcification and high glucose metabolism in the tumor region. **G.** Merged skeletal CT images and images taken after the addition of vasculature contrast showing hypervascularity and calcification of the tumor region. **H.** High-magnification optical NIR imaging showing high signal intensity in the tumor region.

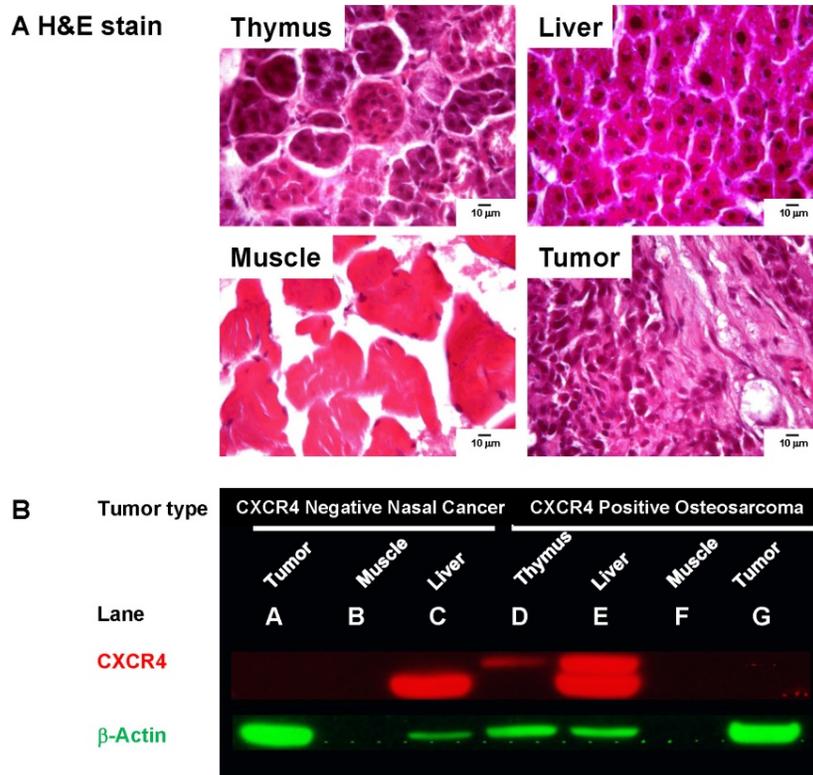


Figure 3. A. Pathology stains verify tissues originating from thymus, liver, muscle, and xenograft tumor. **B.** CXCR4 expression was probed in tissue lysates from mice inoculated with CXCR4 negative nasal cancer cells and CXCR4-positive Saos-2 cells. No CXCR4 was detected in the CXCR4-negative tumor (A), CXCR4-positive tumor (G), or muscle tissue from tumor-bearing mice (B, F). Low molecular weight CXCR4 was detected in the liver of tumor-bearing mice (C and E). High molecular weight CXCR4 was only detected in the thymus (D) and liver (E) of a mouse bearing the CXCR4 positive tumor. β -actin was used as protein loading control.

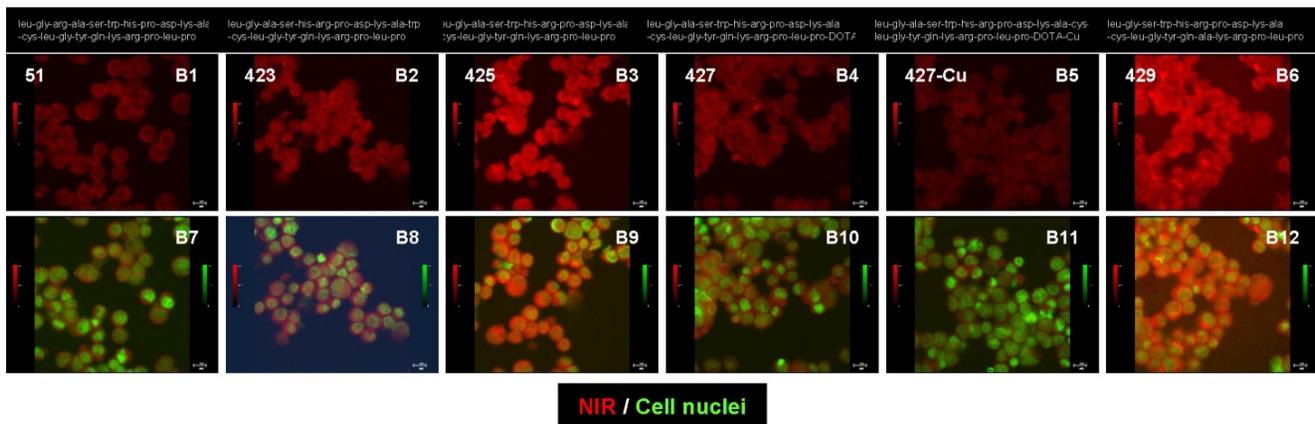


Figure 4. Peptide sequence and structural changes altered the binding of NIR-labeled CXCR4 agents to the Saos-2 cells *in vitro*. The NIR signal intensities are presented at the same scale (B1 to B6) and merged with cell nuclei (B7 to B12) for each of the peptide agents.

ists are being evaluated clinically [13, 15, 20-33]. Therefore, development of a noninvasive method for evaluating and monitoring biological changes in CXCR4 status is vital for both preclinical studies and ongoing clinical trials. Using a human osteosarcoma model, we validated a readily produced peptide agent targeting CXCR4. Using confocal microscopy, we demonstrated that the target-specific component of the CXCR4 peptide agent is important for tumor cell binding, as the NIR dye alone did not bind cells. *In vivo* optical imaging confirmed high NIR signal

intensity within the CXCR4-positive tumor and within CXCR4 receptor-positive organs. Furthermore, we demonstrated that small molecule, target-specific peptide agents in combination with advanced structural, metabolic, and vasculature imaging technologies can be used to define disease status *in vivo*.

The largest challenge for this study was in validating CXCR4 expression in tumor lysates by Western blotting. We selected the antibody used in this study based on its well-established use, published results [34], and availability. Western blot analysis

clearly demonstrated CXCR4 expression in the mouse liver, but did not detect any CXCR4 in the tumors. However, high molecular weight CXCR4 was only detected in the thymus and liver from the mouse with the CXCR4-positive Saos-2 xenograft. This high molecular weight form of CXCR4 was not detected in tissues from the mouse bearing the CXCR4-negative nasal tumor. Results from additional CXCR4 antibodies suggested that the CXCR4 positive osteosarcoma stimulates the host thymus and may produce another form of CXCR4 protein not detected by the currently available CXCR4 antibodies. Despite the failure of the antibody validation step, our peptide-imaging agent has been used to detect CXCR4 in several other disease models, such as leukemia and liver cancer (data not shown). The findings of our Western blot analyses highlight the challenges associated with antibody-based agents and suggest that each target-specific agent exhibits selective binding in different animal models [35-37].

We developed several dozen agents with different sequences and structures, but only presented four modified CXCR4 agents here. The CXCR4 peptide agent used for the *in vivo* studies exhibited the most conserved binding affinity for diverse human disease models. The binding data from the complete set of peptide agents will be summarized in a journal that focuses on chemistry. The binding affinity and signal intensity for these peptide agents varied for each of the cell lines and tumor models studied, confirming that minor structural modifications significantly affect the binding affinity of peptide agents [38]. By including a NIR label on the CXCR4 peptide agent, we were able to combine NIR/single photon emission CT (NIR/ SPECT) and NIR/PET imaging for evaluating the progression of the osteosarcoma xenograft. The results presented here confirm that NIR-labeled peptide agents can be easily modified for disease target specificity and have the potential to be utilized in precision medicine for noninvasive imaging of molecular markers.

Materials and Methods

CXCR4 agent synthesis

(NIR dye- leu-gly-ala-ser-trp-his-arg-pro-asp-lys-ala-cys-leu-gly-tyr-gln-lys-arg-pro-leu-pro-NH₂): d-amino-peptide LGASWHRPDKACLG YQKRPLP (DVI-C11A [39]) was prepared following standard procedures for Fmoc solid-phase peptide synthesis on a Symphony synthesizer (Protein Technologies, Inc., Tucson, AZ). The conjugation of NIR-dye-NHS [40] to the peptide was carried out on the solid support in presence of N, N-diisopropylethylamine (10%) in DMF. The compound was cleaved from the support using trifluoroacetic acid/water/triethylsilane

(94/2/4) and purified by reverse phase HPLC. The product was validated by mass and analytic HPLC. Matrix-assisted laser desorption/ionization (MALDI) for C₁₅₃H₂₂₁N₃₆O₃₃S₄⁺ calculated as 3218.56 [M]⁺, and found to be 3218.56; HPLC (water and acetonitrile containing 0.1% TFA from 10 to 80% in 30 min) retention time was 18.41 min and purity was over 95%. The alternate peptide sequences used in the cell-binding assay were synthesized in the same manner and the sequences were presented in the results.

Tumor cell lines

Saos-2, a metastatic human osteosarcoma cancer cell line that expresses high levels of CXCR4, was purchased from the American Type Culture Collection (ATCC, Manassas, VA). CXCR4 negative nasal cancer cell line SUNE-1 was a kind gift from Sun Yat-sen University. Both cells were cultured in Dulbecco's Modified Eagle's medium supplemented with high glucose and F12 nutrient (Invitrogen, Carlsbad, CA) and 10% fetal bovine serum (HyClone; Thermo Fisher Scientific Inc., Waltham, MA) in a humidified incubator maintained at 37°C with 5% CO₂.

Tumor xenografts

To generate single cells suspensions, Saos-2 cells cultured near confluence were incubated with 0.05% trypsin-EDTA buffer, followed by centrifugation at 130 × g for 5 min. The cell pellet was resuspended in sterile PBS, and then approx. One million tumor cells were implanted subcutaneously into the hind region of four- to six-week-old male athymic nude mice (18-22 g) (Harlan Sprague Dawley, Inc., Indianapolis, IN). Before and after surgery, the mice were housed in a pathogen-free mouse colony and given sterilized pellet chow and sterilized water.

Fluorescent confocal imaging

Cultured tumor cells were harvested and incubated with NIR-labeled CXCR4 agent or NIR free dye for 60 min at 37°C. To fix the cells and stain the nuclei, cells were then washed in PBS and incubated with Sytox green (Molecular Probes; Invitrogen) diluted in 95% ethanol for 15 min at 4°C. Stained cells were mounted onto microscope slides and signal intensities of labeled cells were recorded from one z-stack slice on an Olympus confocal microscope (FluoView 1000; Olympus America, Center Valley, PA). Sytox green signals (ex/em 488/510 nm) were pseudocolored green; CXCR4 agent or NIR dye signals (ex/em 765/810 nm) were pseudocolored red.

In vivo imaging

Five nmol NIR-labeled CXCR4 was injected via the tail vein into nude mice bearing human

osteosarcoma xenografts. Each mouse was imaged for up to 3 days after the injection with a Bruker In-Vivo Multispectral System FX Pro instrument (Bruker Preclinical Imaging, Billerica, MA). For comparative purposes, all images were captured over time using the same standard protocol and were saved as uncompressed 16-bit tagged image file format (TIFF) images for further analysis. Tumor vasculature was assessed by CT imaging (Siemens MicroCAT II; Siemens Medical Solutions, Malvern, PA) after the injection of Ominipaque (GE Healthcare, Princeton, NJ). The glucose metabolic status of tumors was determined by PET imaging (Siemens Inveon) after the injection of ¹⁸F-FDG (Cyclotope, Houston, TX). ImageJ (National Institutes of Health, Bethesda, MD) and Amira (Visage Imaging, Inc., Carlsbad, CA) were used for three-dimensional (3D) reconstructions, volume rendering, and tumor-to-background ratio analysis.

Western blot analysis

Tissues were homogenized in cold RIPA buffer with protease inhibitor cocktails (Sigma-Aldrich, St. Louis, MO). Tissue debris was removed by centrifugation. Equal amounts of 1× Laemmli sample buffer (Bio-Rad Laboratories, Hercules, CA) were added to the samples, and the mixtures were heated to 95°C. The samples were then subjected to sodium dodecyl sulfate polyacrylamide gel electrophoresis (SDS-PAGE) and transferred onto nitrocellulose membranes. Finally, each membrane was incubated with anti-human CXCR4 antibody according to the manufacture instructions (R&D Systems, Minneapolis, MN) for 1 h and developed by using the ECL chemiluminescence detection kit (GE Healthcare Life Sciences, Piscataway, NJ). Membranes were incubated with β-actin antibody (Sigma-Aldrich, St. Louis, MO) as a loading control.

Abbreviations

CT: Computed tomography; FDG or ¹⁸F-FDG: fluoro-deoxy-glucose; MRI: magnetic resonance imaging; NIR: near-infrared; PET: positron emission tomography; SDS-PAGE: sodium dodecyl sulfate polyacrylamide gel electrophoresis; ex: excitation; em: emission; nm: nanometer; DIC: differential interference contrast; GAPDH: glyceraldehyde 3-phosphate dehydrogenases; H&E: hematoxylin and eosin; SPECT: single photo emission computed tomography.

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Authors' contributions statement

All authors read the manuscript and contributed to the final version.

Ethics Statement

All animals were handled in accordance with good animal practice as defined by the relevant national and/or local animal welfare bodies. All animal work was approved by the Wenzhou Medical University Institutional Animal Care and Use Committee. The animal facilities are operated in compliance with the Guide for the Care and Use of Laboratory Animals.

Availability of data and materials

The datasets used and/or analyzed in the current study are available by request from the corresponding author.

Competing Interests

The authors have declared that no competing interest exists.

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